

US009198666B2

(12) United States Patent

Berez et al.

(45) Date of Patent:

(10) **Patent No.:**

US 9,198,666 B2

*Dec. 1, 2015

(54) SYSTEM AND METHOD FOR DELIVERING AND DEPLOYING AN OCCLUDING DEVICE WITHIN A VESSEL

(75) Inventors: Aaron Lee Berez, Menlo Park, CA

(US); Quang Quoc Tran, Redwood

City, CA (US)

(73) Assignee: Covidien LP, Mansfield, MA (US)

(*) Notice: Subject to any disclaimer, the term of this

patent is extended or adjusted under 35 U.S.C. 154(b) by 679 days.

2.6.2.12.(e) 5j 513 days.

This patent is subject to a terminal dis-

claimer.

(21) Appl. No.: 13/550,095

(22) Filed: Jul. 16, 2012

(65) **Prior Publication Data**

US 2012/0283815 A1 Nov. 8, 2012

Related U.S. Application Data

- (60) Continuation of application No. 12/420,383, filed on Apr. 8, 2009, now Pat. No. 8,236,042, which is a division of application No. 11/136,398, filed on May 25, 2005, now Pat. No. 8,147,534.
- (51) Int. Cl.

 A61F 2/06 (2013.01)

 A61B 17/12 (2006.01)

 (Continued)
- (52) **U.S. CI.**CPC *A61B 17/12022* (2013.01); *A61B 17/12118*(2013.01); *A61F 2/966* (2013.01);
 (Continued)
- (58) Field of Classification Search

CPC ... A61B 17/12118; A61F 2/962; A61F 2/966; A61F 2/9665; A61F 2002/823; A61F 2/95; A61F 2002/9505–2002/9511; A61F 2002/9534; A61F 2002/9522 USPC 606/191, 192, 194, 195, 198; 623/1.11, 623/1.12 See application file for complete search history.

(56) References Cited

U.S. PATENT DOCUMENTS

4,321,711 A 3/1982 Mano 4,503,569 A 3/1985 Dotter (Continued)

FOREIGN PATENT DOCUMENTS

EP 418677 3/1991 EP 442657 8/1991 (Continued)

OTHER PUBLICATIONS

Hill, et al., "Initial Results of the Amplatzer Vascular Plug in the Treatment of Congenital Heart Disease, Business Briefing" US Cardiology, 2004.

(Continued)

Primary Examiner — Todd Manahan

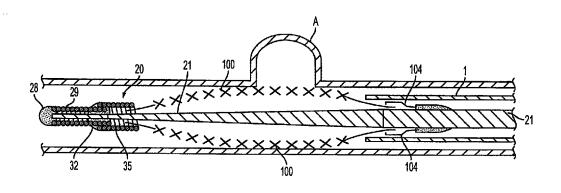
Assistant Examiner — Charles Wei

(74) Attorney, Agent, or Firm — Mark J. Kertz, Esq.

(57) ABSTRACT

A system and method for deploying an occluding device that can be used to remodel an aneurysm within the vessel by, for example, neck reconstruction or balloon remodeling. The system comprises an introducer sheath and an assembly for carrying the occluding device. The assembly includes an elongated flexible member having an occluding device retaining member for receiving a first end of the occluding device, a proximally positioned retaining member for engaging a second end of the occluding device and a support surrounding a portion of the elongated flexible member over which the occluding device can be positioned.

18 Claims, 9 Drawing Sheets



US 9,198,666 B2Page 2

(51)	T			5 605 400		10/1005	TT 1
(51)	Int. Cl.			5,695,499			Helgerson et al.
	A61F 2/966		(2013.01)	5,700,269 5,702,418			Pinchuk et al. Ravenscroft
	A61F 2/82		(2013.01)	5,702,418		1/1998	
(52)	U.S. Cl.			5,709,702			Lukic et al.
(52)			(1D2017/1207/2012 01) 1/1D	5,725,552			Kotula et al.
	CPC		1B2017/1205 (2013.01); A61B	5,725,570		3/1998	
		2017/12	<i>054</i> (2013.01); <i>A61F 2002/823</i>	5,725,571		3/1998	Imbert et al.
		(2013.0)	1); A61F 2002/9665 (2013.01)	5,733,294	A	3/1998	Forber et al.
		`		5,733,327			Igaki et al.
(56)		Referen	ces Cited	5,735,859			Fischell et al.
()				5,741,325			Chaikof et al.
	U.S.	PATENT	DOCUMENTS	5,741,333		4/1998	
				5,749,883			Halpern Var. et al
	4,512,338 A	4/1985	Balko et al.	5,749,891 5,749,919		5/1998	Ken et al.
	4,538,622 A	9/1985	Samson et al.	5,749,920			Quiachon et al.
	4,580,568 A		Gianturco	5,769,884			Solovay
	4,655,771 A		Wallsten	5,769,885			Quiachon et al.
	4,733,665 A		Palmaz	5,776,099	A	7/1998	Tremulis
	4,768,507 A	9/1988 10/1988	Fischell et al.	5,776,140	A		Cottone
	4,776,337 A 4,954,126 A		Wallsten	5,776,141			Klein et al.
	4,998,539 A		Delsanti	5,776,142			Gunderson
	5,011,488 A		Ginsburg	5,782,909		8/1998	Quiachon et al.
	5,026,377 A		Burton et al.	5,797,952 5,800,518			Piplani et al.
	5,035,706 A	7/1991	Giantureo et al.	5,800,318			Shaknovich
	5,061,275 A		Wallsten et al.	5,810,837			Hofmann et al.
	5,064,435 A	11/1991		5,814,062			Sepetka et al.
	5,108,416 A		Ryan et al.	5,817,102			Johnson et al.
	5,147,370 A *		McNamara et al 623/1.11	5,824,039	A	10/1998	Piplani et al.
	5,160,341 A 5,180,368 A		Brenneman et al. Garrison	5,824,041			Lenker et al.
	5,192,297 A	3/1993		5,824,044			Quiachon et al.
	5,201,757 A		Heyn et al.	5,824,058			Ravenscroft et al.
	5,209,731 A		Sterman et al.	5,833,632 5,836,868			Jacobsen et al. Ressemann et al.
	5,222,971 A		Willard et al.	5,846,261			Kotula et al.
	5,242,399 A		Lau et al.	5,868,754			Levine et al.
	5,246,420 A		Kraus et al.	5,873,907			Frantzen
	5,246,445 A		Yachia et al.	5,888,201		3/1999	Stinson et al.
	5,334,210 A		Gianturco Lau et al.	5,902,266			Leone et al.
	5,344,426 A 5,360,443 A		Barone et al.	5,906,640		5/1999	Penn et al.
	5,378,239 A		Termin et al.	5,911,717		6/1999	Jacobsen et al.
	5,382,259 A		Phelps et al.	5,916,194 5,916,235		6/1999	Jacobsen et al. Guglielmi
	5,401,257 A	3/1995	Chevalier, Jr. et al.	5,919,204			Lukic et al.
	5,405,380 A		Gianotti et al.	5,925,060		7/1999	
	5,415,637 A		Khosravi	5,928,260		7/1999	Chin et al.
	5,421,826 A 5,423,849 A		Crocker et al. Engelson et al.	5,935,148		8/1999	
	5,445,646 A		Euteneuer et al.	5,944,726		8/1999	Blaeser et al.
	5,449,372 A		Schmaltz et al.	5,944,738		8/1999	Amplatz et al.
	5,458,615 A		Klemm et al.	5,951,599		9/1999	McCrory
	5,476,505 A	12/1995		5,957,973 5,957,974			Quiachon et al. Thompson et al.
	5,480,423 A	1/1996	Ravenscroft et al.	5,964,797		10/1999	
	5,484,444 A		Braunschweiler et al.	5,972,015			Scribner et al.
	5,489,295 A		Piplani et al.	5,980,530			Willard et al.
	5,503,636 A		Schmitt et al.	5,980,533		11/1999	Holman
	5,507,768 A 5,522,822 A		Lau et al. Phelps et al.	5,980,554			Lenker et al.
	5,534,007 A		St. Germain et al.	5,984,929			Bashiri et al.
	5,545,209 A		Roberts et al.	6,014,919	A		Jacobsen et al.
	5,549,635 A	8/1996		6,015,432 6,017,319	A		Rakos et al. Jacobsen et al.
	5,562,641 A	10/1996	Flomenblit et al.	6,019,778			Wilson et al.
	5,562,728 A		Lazarus et al.	6,019,786	A		Thompson
	5,591,225 A	1/1997		6,022,369			Jacobsen et al.
	5,599,291 A		Balbierz et al.	6,024,754			Engelson
	5,607,466 A		Imbert et al.	6,024,763			Lenker et al.
	5,609,625 A 5,626,602 A		Piplani et al. Gianotti et al.	6,027,516			Kolobow et al.
	5,626,602 A 5,628,783 A		Quiachon et al.	6,033,423			Ken et al.
	5,632,772 A		Alcime et al.	6,036,720			Abrams et al.
	5,636,641 A		Fariabi	6,039,758			Quiachon et al.
	5,643,278 A	7/1997		6,042,589			Marianne
	5,662,703 A		Yurek et al.	6,051,021		4/2000	
	5,667,522 A		Flomenblit et al.	6,056,993			Leidner et al.
	5,674,276 A		Andersen et al.	6,063,070 6,063,104		5/2000	Villar et al.
	5,683,451 A 5,690,120 A		Lenker et al. Jacobsen et al.	6,063,111			Hieshima et al.
	5,690,644 A		Yurek et al.	6,068,634			Lorentzen Cornelius et al.
	,, 			,,			

US 9,198,666 B2Page 3

(56) Referen	nces Cited	6,395,022 B1	5/2002 6/2002	Piplani et al.
U.S. PATENT	DOCUMENTS	6,398,802 B1 6,409,683 B1		Fonseca et al.
		6,413,235 B1	7/2002	
	Levine et al.	6,416,536 B1 6,428,489 B1	7/2002 8/2002	Jacobsen et al.
	Limon et al. Ken et al.	6,428,558 B1		Jones et al.
	Brown et al.	6,432,130 B1		Hanson
	Callister et al.	6,440,088 B1 6,443,971 B1		Jacobsen et al. Boylan et al.
6,102,942 A 8/2000 6,113,607 A 9/2000	Aharı Lau et al.	6,443,979 B1		Stalker et al.
6,123,712 A 9/2000	Di Caprio et al.	6,447,531 B1		Amplatz
6,123,715 A 9/2000	Amplatz	6,451,025 B1* 6,454,780 B1		Jervis 606/108 Wallace
	Lenker et al. Piplani et al.	6,454,999 B1		Farhangnia et al.
	Esch et al.			Bashiri et al.
6,139,564 A 10/2000				Jacobsen et al. Hebert et al.
6,146,415 A 11/2000 6,149,680 A 11/2000	Fitz Shelso et al.			Cornish et al.
	Lesh et al.	6,503,450 B1	1/2003	Afzal et al.
6,165,178 A 12/2000	Bashiri et al.	6,506,204 B2		Mazzocchi
	Kupiecki et al. Ken et al.	6,511,468 B1 6,514,261 B1		Cragg et al. Randall et al.
, ,	Frantzen	6,520,983 B1	2/2003	Colgan et al.
6,168,622 B1 1/2001	Mazzocchi	6,524,299 B1		Tran et al.
	Jacobsen et al.	6,527,763 B2 6,533,811 B1		Esch et al. Ryan et al.
	Horton et al. Ken et al.	6,540,778 B1		Piplani et al.
	Piplani et al.	6,547,779 B2		Levine et al.
	Parodi	6,547,804 B2 6,551,303 B1		Porter et al. Van Tassel et al.
	Hebert et al. Quiachon et al.	6,572,646 B1		Boylan et al.
	Piplani et al.	6,576,006 B2		Limon et al.
	Piplani et al.	6,579,303 B2 6,582,460 B1	6/2003	Amplatz
	Jacobsen et al. Forber	6,585,748 B1	7/2003	
	Baker et al.	6,589,236 B2		Wheelock et al.
	Ressemann et al.	6,589,256 B2 6,589,265 B1	7/2003	Forber Palmer et al.
	Piplani et al. Deem et al.	6,589,273 B1		McDermott
	Quiachon et al.	6,592,616 B1		Stack et al.
6,241,758 B1 6/2001	Čox	6,599,308 B2 6,602,280 B2		Amplatz Chobotov
	Piplani et al. Stinson	6,605,102 B1		Mazzocchi et al.
	Ravenscroft et al.	6,605,110 B2		Harrison
6,260,458 B1 7/2001	Jacobsen et al.	6,605,111 B2		Bose et al. Hayashi et al.
	Marotta et al. Herweck et al.	6,607,539 B1 6,607,551 B1		Sullivan et al.
6,280,465 B1 8/2001		6,613,074 B1	9/2003	Mitelberg et al.
6,287,331 B1 9/2001		6,613,075 B1		Healy et al. Thompson et al.
6,290,721 B1 9/2001 6,302,810 B2 10/2001		6,623,518 B2 6,626,939 B1		Burnside et al.
	Limon et al.	6,635,068 B1	10/2003	Dubrul et al.
	Wallace et al.			Kupiecki
	Monroe et al. Quiachon et al.		11/2003 11/2003	Campbell et al.
	Abrams	6,652,508 B2	11/2003	Griffin et al.
6,342,068 B1 1/2002	Thompson			VanTassel et al. Ravenscroft et al.
6,344,041 B1 2/2002 6,344,048 B1 2/2002	Kupiecki et al. Chin et al.			Denardo et al.
	Greenhalgh	6,660,024 B1	12/2003	Flaherty et al.
6,348,063 B1 2/2002	Yassour et al.			Quiachon et al. Bose et al.
6,350,199 B1 2/2002 6,350,270 B1 2/2002	Williams et al.			Wallace et al.
	Lenker et al.	6,669,721 B1	12/2003	Bose et al.
6,355,061 B1 3/2002	Quiachon et al.	6,673,089 B1 6,673,100 B2		Yassour et al. Diaz et al.
	Amplatz	6,679,893 B1	1/2004	
	Piplani et al.	6,682,546 B2	1/2004	Amplatz
6,371,928 B1 4/2002	Mcfann et al.	6,682,557 B1		Quiachon et al.
	Gifford et al.	6,685,735 B1 6,689,162 B1	2/2004	Ahari Thompson
6,375,670 B1 4/2002 6,375,676 B1 4/2002	Greenhalgh Cox	6,689,486 B2		Ho et al.
6,379,618 B1 4/2002	Piplani et al.	6,699,274 B2	3/2004	Stinson
	Yurek et al.	6,709,454 B1		Cox et al.
6,383,174 B1 5/2002 6,387,118 B1 5/2002	Eder Hanson	6,712,834 B2 6,716,238 B2	3/2004 4/2004	Yassour et al.
	Greenhalgh	6,716,238 B2 6,726,700 B1	4/2004	
	Dwyer et al.	6,730,108 B2		Van Tassel et al.

US 9,198,666 B2

Page 4

(56) Referen	nces Cited	7,294,137 B2 7,294,146 B2		Rivelli, Jr. et al. Chew et al.
U.S. PATENT	DOCUMENTS	7,300,456 B2	11/2007	Andreas et al.
		7,300,460 B2 7,306,624 B2		Levine et al. Yodfat et al.
	Lashinski et al. Yodfat et al.	7,309,351 B2	12/2007	Escamilla et al.
	Yodfat et al.	7,311,031 B2		McCullagh et al.
	Dwyer et al.	7,320,702 B2 7,331,973 B2		Hammersmark et al. Gesswein et al.
	Sepetka et al. Gupta et al.	7,331,976 B2		McGuckin, Jr. et al.
6,755,855 B2 6/2004	Yurek et al.	7,331,980 B2		Dubrul et al.
	Leffel et al. Quiachon et al.	7,331,985 B2 7,338,518 B2		Thompson et al. Chobotov
	Dwyer et al.	7,419,503 B2		Pulnev et al.
	Chin et al.	7,468,070 B2 7,470,282 B2	12/2008 12/2008	Henry et al.
	Hebert et al. Jones et al.	7,473,271 B2		Gunderson
6,811,560 B2 11/2004	Jones et al.	7,491,224 B2		Cox et al.
	Baker et al. Douk et al.	7,578,826 B2 7,597,704 B2		Gandhi et al. Frazier et al.
6,833,003 B2 12/2004		7,785,361 B2*	8/2010	Nikolchev et al 623/1.11
	Rabkin et al.	7,862,602 B2 8,114,154 B2		Licata et al. Righini et al.
	Saadat Hijlkema et al.	8,147,534 B2		Berez et al.
6,860,893 B2 3/2005	Wallace et al.	8,192,480 B2		Tieu et al.
	Stack et al. Baker et al.	8,206,431 B2 8,236,042 B2		Seppala et al. Berez et al.
	Douk et al.	8,257,421 B2	9/2012	Berez et al.
	Yassour et al.	8,267,985 B2 8,273,101 B2		Garcia et al. Garcia et al.
	Dworschak et al. Feeser et al.	2001/0000797 A1		Mazzocchi
6,936,055 B1 8/2005	Ken et al.	2001/0012949 A1	8/2001	
	Escamilla et al. Jones et al.	2001/0012961 A1 2001/0049547 A1	12/2001	Deem et al. Moore
	Shah et al.	2002/0013618 A1	1/2002	Marotta et al.
	Hebert et al.	2002/0062091 A1 2002/0078808 A1		Jacobsen et al. Jacobsen et al.
	Hebert et al. van der Burg et al.	2002/0078808 AT 2002/0087119 A1	7/2002	
6,994,717 B2 2/2006	Konya et al.	2002/0099405 A1		Yurek et al.
6,994,721 B2 2/2006 7,001,422 B2 2/2006	Israel Escamilla et al.	2002/0120323 A1 2002/0143384 A1	8/2002 10/2002	Thompson et al. Ozasa
	Thompson et al.	2002/0165572 A1	11/2002	Saadat
	Welch	2002/0169473 A1 2002/0188341 A1	11/2002 12/2002	Sepetka et al.
	Hemerick et al. Greene, Jr. et al.	2003/0028209 A1		Teoh et al.
7,037,330 B1 5/2006	Rivelli, Jr. et al.	2003/0057156 A1		Peterson et al.
	Chobotov Nishri et al.	2003/0069522 A1 2003/0100945 A1		Jacobsen et al. Yodfat et al.
	Rabkin et al.	2003/0109887 A1	6/2003	Galdonik et al.
	Avellanet et al.	2003/0135258 A1 2003/0149465 A1		Andreas et al. Heidner et al.
	Rapaport et al. Heath	2003/0143465 A1 2003/0163155 A1		Haverkost et al.
	Bjorklund et al.	2003/0163156 A1	8/2003	Hebert et al.
	Vrba et al. Quiachon et al.	2003/0171739 A1 2003/0195553 A1		Murphy et al. Wallace et al.
	Randall et al.	2003/0199913 A1	10/2003	Dubrul et al.
	Sequin et al.	2003/0208256 A1 2003/0216693 A1		DiMatteo et al. Mickley
	van der Burg et al. Abrams et al.	2004/0024416 A1	2/2004	Yodfat et al.
7,137,990 B2 11/2006	Hebert et al.	2004/0044391 A1 2004/0044395 A1	3/2004	Porter Nelson
	Baker et al. Widenhouse	2004/0044393 A1 2004/0049204 A1		Harari et al.
7,169,172 B2 1/2007	Levine et al.	2004/0049256 A1	3/2004	
	Obara Colgan et al.	2004/0059407 A1 2004/0073300 A1		Escamilla et al. Chouinard et al.
	Avellanet et al.	2004/0078071 A1	4/2004	Escamilla et al.
7,195,639 B2 3/2007	Quiachon et al.	2004/0093010 A1 2004/0093063 A1*		Gesswein et al. Wright et al 623/1.12
	Jones et al. Diaz et al.	2004/0093063 A1 2004/0122468 A1		Yodfat et al 023/1.12
7,201,769 B2 4/2007	Jones et al.	2004/0127912 A1*	7/2004	
	Thompson McCullagh et al	2004/0138733 A1 2004/0143286 A1		Weber et al. Johnson et al.
	McCullagh et al. Chin et al.	2004/0143280 A1 2004/0186551 A1		Kao et al.
7,232,461 B2 6/2007	Ramer	2004/0186562 A1	9/2004	Cox
	Van Tassel et al. Wright et al.	2004/0193178 A1 2004/0193179 A1		Nikolchev Nikolchev
	Wright et al. Nishri et al.	2004/01931/9 A1 2004/0193206 A1		Gerberding et al.
7,279,005 B2 10/2007	Stinson	2004/0199243 A1	10/2004	Yodfat
7,279,208 B1 10/2007	Goffena et al.	2004/0204749 A1	10/2004	Gunderson

US 9,198,666 B2

Page 5

(56)	Referen	ces Cited		82154 A1		Tseng et al.
U.S.	. PATENT	DOCUMENTS	2008/01	97495 A1 19886 A1	5/2008	Feller, III et al. Greenhalgh et al.
2004/0215332 A1	10/2004	Ewid		54286 A1 95139 A1		Abbott et al. Donald et al.
2004/0213332 A1 2004/0220585 A1		Nikolchev	2008/02	08320 A1	8/2008	Tan-Malecki et al.
2005/0010281 A1		Yodfat et al.		19533 A1 21600 A1		Grigorescu Dieck et al.
2005/0033408 A1 2005/0033409 A1		Jones et al. Burke et al.		21666 A1*		Licata et al 623/1.22
2005/0049668 A1		Jones et al.		55654 A1		Hebert et al.
2005/0049670 A1		Jones et al.		52590 A1 59774 A1	10/2008	Murray Garcia et al.
2005/0090890 A1 2005/0096728 A1	5/2005	Wu et al. Ramer		81350 A1	11/2008	Sepetka et al.
2005/0096732 A1	5/2005	Marotta et al.		00667 A1		Hebert et al.
2005/0107823 A1 2005/0131523 A1		Leone et al. Bashiri et al.		19533 A1 24202 A1	12/2008 1/2009	Dave et al.
2005/0137680 A1		Ortiz et al.	2009/00	24205 A1	1/2009	Hebert et al.
2005/0209672 A1		George et al.		25820 A1 30496 A1	1/2009 1/2009	Adams Kaufmann et al.
2005/0228434 A1 2005/0246010 A1		Amplatz et al. Alexander et al.		30497 A1		Metcalf et al.
2005/0267568 A1		Berez et al.		82803 A1	3/2009	Adams et al.
2005/0283220 A1		Gobran et al. Betelia et al.		05802 A1 05803 A1	4/2009 4/2009	Henry et al. Shelso
2005/0283222 A1 2005/0288764 A1		Snow et al.	2009/01	12251 A1	4/2009	Qian et al.
2005/0288766 A1	12/2005	Plain et al.		25093 A1 38065 A1		Hansen Zhang et al.
2006/0036309 A1 2006/0052815 A1		Hebert et al. Fitz et al.		53986 A1	6/2009	
2006/0052815 A1 2006/0052816 A1		Bates et al.		92536 A1		Berez et al.
2006/0058865 A1		Case et al.		10047 A1 54978 A1	8/2009 10/2009	Amplatz et al. Dieck et al.
2006/0064151 A1 2006/0089703 A1		Guterman et al. Escamilla et al.		70974 A1	10/2009	
2006/0095213 A1		Escamilla et al.		75974 A1		Marchand et al.
2006/0111771 A1		Ton et al.		87241 A1 87288 A1		Berez et al. Berez et al.
2006/0116714 A1 2006/0116750 A1		Sepetka et al. Hebert et al.		87292 A1		Becking et al.
2006/0155323 A1	7/2006	Porter et al.		92348 A1		Berez et al.
2006/0167494 A1 2006/0184238 A1		Suddaby Kaufmann et al.		18947 A1 19017 A1	12/2009 12/2009	
2006/0184238 A1 2006/0190076 A1	8/2006		2010/003	30220 A1	2/2010	Truckai et al.
2006/0206200 A1		Garcia et al.		59948 A1 52767 A1	3/2010 6/2010	Veznedaroglu et al. Greenhalgh et al.
2006/0206201 A1 2006/0212127 A1		Garcia et al. Karabey et al.		58204 A1		Tieu et al.
2006/0235464 A1		Avellanet et al.		05606 A1	12/2010	
2006/0235501 A1	10/2006			31948 A1 13447 A1	12/2010	Turovskiy et al. Strauss et al.
2006/0247680 A1 2006/0271149 A1		Amplatz et al. Berez et al.	2012/004	41470 A1	2/2012	Shrivastava et al.
2006/0271153 A1	11/2006	Garcia et al.		41474 A1		Eckhouse et al.
2007/0021816 A1 2007/0043419 A1	1/2007	Rudin Nikolchev et al.		55720 A1 21095 A1		Strauss et al. Berez et al.
2007/0055339 A1		George et al.	2012/02	77784 A1	11/2012	Berez et al.
2007/0073379 A1	3/2007			83765 A1 83815 A1		Berez et al. Berez et al.
2007/0088387 A1 2007/0100414 A1		Eskridge et al. Licata et al.		14380 A1		Quadri et al.
2007/0106311 A1	5/2007	Wallace et al.		72976 A1		Garcia et al.
2007/0112415 A1 2007/0119295 A1		Bartlett McCullagh et al.		EODEL		AVE DOCK DOCK DOCK
2007/0119293 A1 2007/0123969 A1		Gianotti		FOREIG	JN PATE.	NT DOCUMENTS
2007/0162104 A1	7/2007		EP	69	6447 A2	2/1996
2007/0167980 A1 2007/0191884 A1		Figulla et al. Eskridge et al.	EP		9098	12/2003
2007/0198075 A1	8/2007	Levy	EP EP		0219 1148	3/2004 2/2006
2007/0198076 A1		Hebert et al.	EP		3 404	1/2010
2007/0203559 A1 2007/0203563 A1		Freudenthal et al. Hebert et al.	EP JP		3 460	1/2010
2007/0203567 A1	8/2007	Levy	JP JP		8216 A 9901 A	12/1998 11/1999
2007/0208376 A1 2007/0221230 A1	9/2007	Meng Thompson et al.	JP	2001-50	9412 A	7/2001
2007/0221230 A1 2007/0225760 A1		Moszner et al.	JP WO	2005-07 WO-95/0	4230 A	3/2005 4/1995
2007/0225794 A1		Thramann et al.	WO	WO-93/0		7/1997
2007/0239261 A1 2007/0265656 A1		Bose et al. Amplatz et al.	WO	WO-98/0	9583 A2	3/1998
2007/0270902 A1	11/2007	Slazas et al.	WO WO	WO-99/0 WO-99/0		1/1999 1/1999
2007/0288083 A1	12/2007		WO	WO-99/0	5977	2/1999
2007/0299500 A1 2007/0299501 A1		Hebert et al. Hebert et al.	WO	WO-99/4		10/1999
2007/0299502 A1		Hebert et al.	WO WO	WO-99/6 WO-00/1		12/1999 3/2000
2008/0003354 A1	1/2008		WO	WO-01/0	5331	1/2001
2008/0021535 A1 2008/0039933 A1		Leopold et al. Yodfat et al.	WO WO	WO-01/9 WO-02/0		12/2001 1/2002
2000/00 <i>33333</i> A1	2/2000	Tourat et al.	*** •	VV O-02/0	0137	1/2002

(56)	References Cited					
	FOREIGN PATE	NT DOCUMENTS				
WO WO	WO-02/28320 A2 WO-02/056798 A2	4/2002 7/2002				
WO	WO-02/060345 A2	8/2002				
WO	WO-02/071977 A2	9/2002				
WO	WO-03/007840	1/2003				
WO	WO-03/022124	3/2003				
WO	WO-03/049600	6/2003				
WO	WO-2004/010878 A1	2/2004				
WO	WO-2004/030575	4/2004				
WO	WO-2004/066809 A2	8/2004				
WO	WO-2004/087006 A3	11/2004				
WO	WO-2005/018728 A2	3/2005				
WO	WO-2005/030093	4/2005				
WO	WO-2005/115118	12/2005				
WO	WO-2005/117718	12/2005				
WO	WO-2006/026744	3/2006				
WO	WO-2006/052322 A2	5/2006				
WO	WO-2006/091891 A2	8/2006				
WO	WO-2006/127005	11/2006				
WO	WO-2007/121405	10/2007				
WO	WO-2008/022327 A2	2/2008				
WO	WO-2008/151204	12/2008				
WO	WO-2008/157507 A2	12/2008				
WO	WO-2009/134337	11/2009				
WO	WO-2010/030991	3/2010				
WO	WO-2011/130081 A1	10/2011				

OTHER PUBLICATIONS

Ronen, "Amplatzer Vascular Plug Case Study, Closure of Arteriovenous Fistula Between Deep Femoral Artery and Superficial Femoral Vein," AGA Medical Corporation, May 2007.

Benndorf et al., "Treatment of ruptured dissecting vertebral artery anneurysm with double stent placement: case report," Am J Neuroradiol., Dec. 2001, vol. 22, No. 10, pp. 1844-1848.

Brilstra et al., Treatment of Intercranial Aneurysms by Emboloization with Coils: A Systematic Review, Stroke, 1999, vol. 30, pp. 470-476.

Ferguson, "Physical Factors in the Initiation, Growth and Rupture of Human Intracranial Saccular Aneurysms," J Neurosurg., 1972, vol. 37, pp. 666-677.

Geremia et al., "Embolization of experimentally created aneurysms with intravascular stent devices," Am J. Neuroradiol., Aug. 1994, vol. 15, No. 7, pp. 1223-1231.

Geremia et al., "Occlusion of experimentally created fusiform aneurysms with porous metallic stents," Am J Neuroradiol., Apr. 2000, vol. 4, pp. 739-745.

Lanzino et al., "Efficancy and current limitiations of intravascular stents for intracranial internal cartoid, vertebral, and basilar artery aneurysms," J Neurosurg., 1999, vol. 91, pp. 538-546.

Lieber et al, "The Physics of Endoluminal Stenting in the Treatment of Cerebrovascular Aneurysms," Neurological Research, 2002, vol. 24, Supplement 1, pp. S32-S42.

Lieber et al., "Alteration of Hemodynamics in Aneurysm Models by Stenting: Influence of Stent Porosity," Ann of Biomedical Eng., 1997, vol. 25, p. 460.

Moss, "Vascular Occulusion with a Balloon-Expandable Stent Occluder," Radiology, vol. 191, No. 2, May 1994, pp. 483-486.

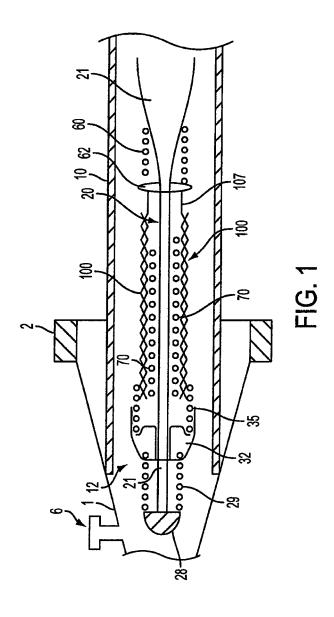
Pereira, "History of Endovascular Aneurysms Occlusion in Management of Cerebral Aneurysms," Eds: Le Roux et al., 2004, pp. 11-26. Qureshi, "Endovascular Treatment of Cerebrovascular Diseases and Intracranial Neoplasms," The Lancet, Mar. 2004, vol. 363, pp. 804-813

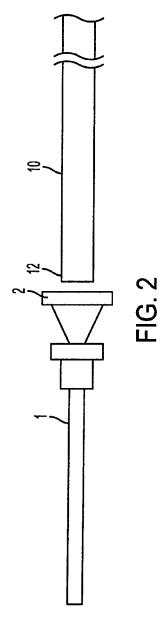
Steiger, "Pathophysiology of Development and Rupture of Cerebral Aneurysms," Acta Neurochir Suppl., 1990, vol. 48, pp. 1-57.

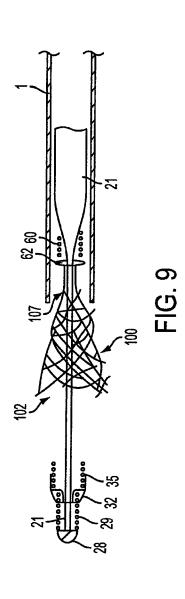
Tenaglia, A. "Ultrasound Guide Wire-Directed Stent Deployment," Duke Univ. Medical Center, Department of Medicine, Am Heart J., 1993.

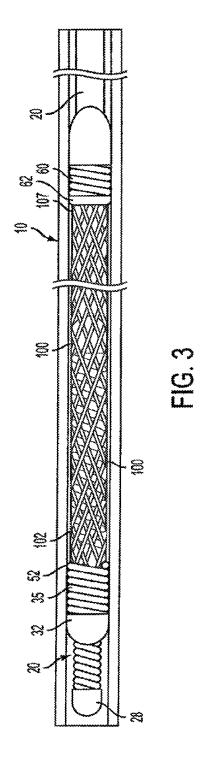
Yu et al., "A steady flow analysis on the stented and non-stented s dewall aneurysm models," Med Eng Phys., Apr. 1999, vol. 21, No. 3, 133-141.

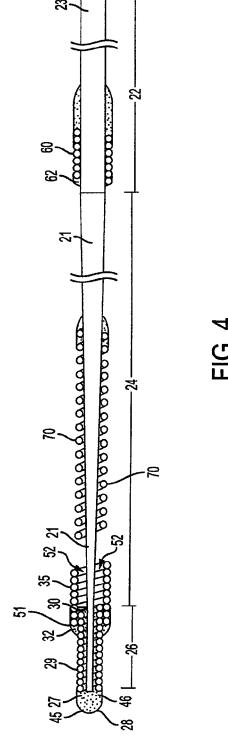
^{*} cited by examiner

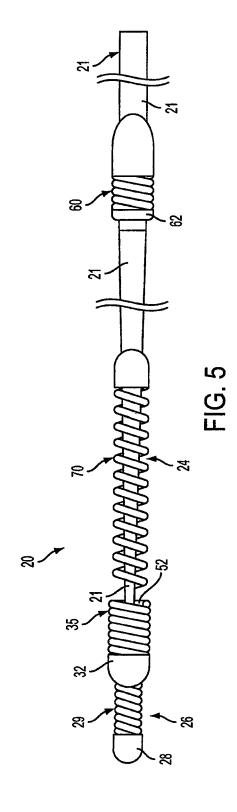


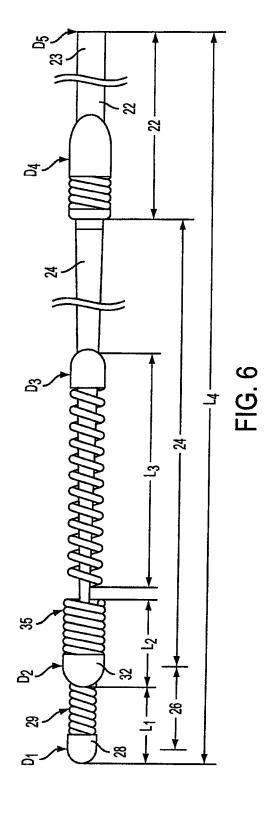


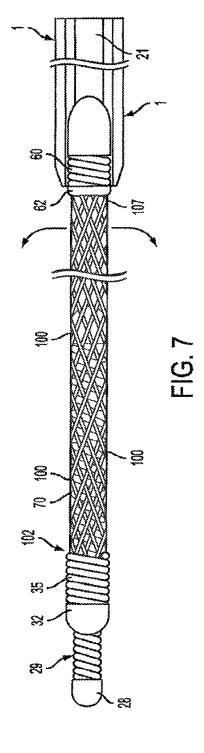


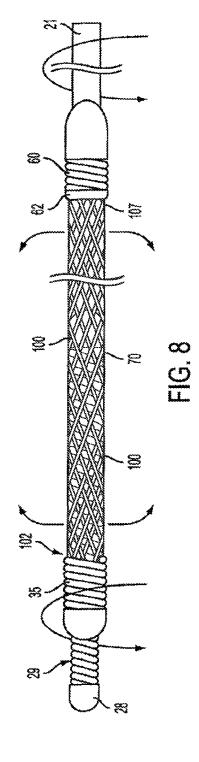


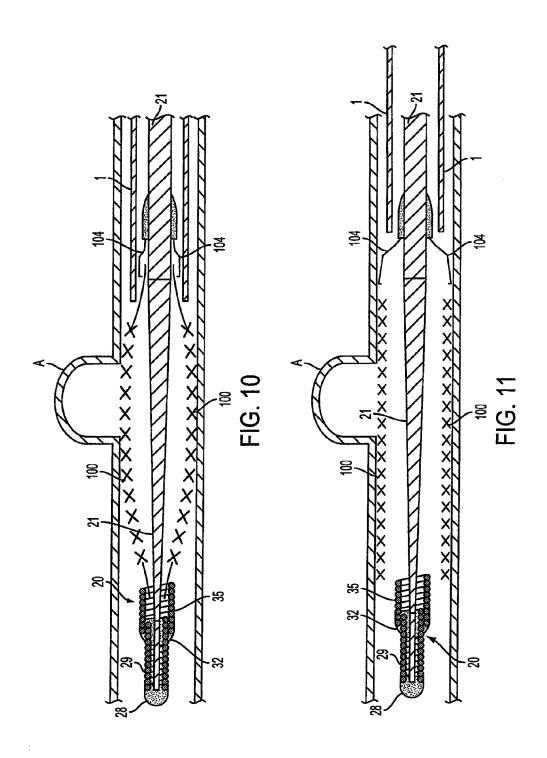












SYSTEM AND METHOD FOR DELIVERING AND DEPLOYING AN OCCLUDING DEVICE WITHIN A VESSEL

CROSS-REFERENCE TO RELATED APPLICATIONS

This application is a continuation of U.S. patent application Ser. No. 12/420,383, filed Apr. 8, 2009, which is a divisional of U.S. patent application Ser. No. 11/136,398, filed May 25, 2005, both of which are expressly incorporated herein by reference in their entireties.

FIELD

The invention generally relates to a system and method for delivering and deploying a medical device within a vessel, more particularly, it relates to a system and method for delivering and deploying an endoluminal therapeutic device within the vasculature of a patient to embolize and occlude aneurysms, particularly cerebral aneurysms.

BACKGROUND

Walls of the vasculature, particularly arterial walls, may develop areas of pathological dilatation called aneurysms. As is well known, aneurysms have thin, weak walls that are prone to rupturing. Aneurysms can be the result of the vessel wall being weakened by disease, injury or a congenital abnormality. Aneurysms could be found in different parts of the body with the most common being abdominal aortic aneurysms and brain or cerebral aneurysms in the neurovasculature. When the weakened wall of an aneurysm ruptures, it can result in death, especially if it is a cerebral aneurysm that ruptures.

Aneurysms are generally treated by excluding the weak-ened part of the vessel from the arterial circulation. For treating a cerebral aneurysm, such reinforcement is done in many ways including: (i) surgical clipping, where a metal clip is secured around the base of the aneurysm; (ii) packing the aneurysm with small, flexible wire coils (micro-coils); (iii) using embolic materials to "fill" an aneurysm; (iv) using 40 detachable balloons or coils to occlude the parent vessel that supplies the aneurysm; and (v) intravascular stenting.

Intravascular stents are well known in the medical arts for the treatment of vascular stenoses or aneurysms. Stents are prostheses that expand radially or otherwise within a vessel or 45 lumen to provide support against the collapse of the vessel. Methods for delivering these intravascular stents are also well known.

In conventional methods of introducing a compressed stent into a vessel and positioning it within in an area of stenosis or an aneurysm, a guiding catheter having a distal tip is percutaneously introduced into the vascular system of a patient. The guiding catheter is advanced within the vessel until its distal tip is proximate the stenosis or aneurysm. A guidewire positioned within an inner lumen of a second, inner catheter and the inner catheter are advanced through the distal end of the guiding catheter. The guidewire is then advanced out of the distal end of the guidewire carrying the compressed stent is positioned at the point of the lesion within the vessel. Once the compressed stent is located at the lesion, the stent may be released and expanded so that it supports the vessel.

SUMMARY

Aspects of the present invention include a system and method of deploying an occluding device within a vessel. The

2

occluding device can be used to remodel an aneurysm within the vessel by, for example, neck reconstruction or balloon remodeling. The occluding device can be used to form a barrier that retains occlusion material such as a well known coil or viscous fluids, such as "ONYX" by Microtherapeutics, within the aneurysm so that introduced material will not escape from within the aneurysm. Also, during deployment, the length of the occluding device can be adjusted in response to friction created between the occluding device and an inner surface of a catheter. When this occurs, the deployed length and circumferential size of the occluding device can be changed as desired by the physician performing the procedure.

An aspect of the present invention includes a system for supporting and deploying an occluding device. The system comprises an introducer sheath and an assembly for carrying the occluding device. The assembly includes an elongated flexible member having an occluding device retaining member for receiving a first end of the occluding device, a proximally positioned retaining member for engaging a second end of the occluding device and a support surrounding a portion of the elongated flexible member over which the occluding device can be positioned.

Another aspect of the present invention includes a system for supporting and deploying an occluding device. The system comprises an assembly for carrying the occluding device. The assembly comprises an elongated member including a flexible distal tip portion, a retaining member for receiving a first end of the occluding device, and a support surrounding a portion of the elongated flexible member for supporting the occluding device.

A further aspect of the present invention comprises a method of introducing and deploying an occluding device within a vessel. The method includes the steps of introducing an elongated sheath including an introducer sheath carrying a guidewire assembly into a catheter and advancing the guidewire assembly out of the sheath and into the catheter. The method also includes the steps of positioning an end of the catheter proximate an aneurysm, advancing a portion of the guidewire assembly out of the catheter and rotating a portion of the guidewire assembly while deploying the occluding device in the area of the aneurysm.

BRIEF DESCRIPTION OF THE FIGURES

FIG. 1 is a cross section of an occluding device delivery assembly and occluding device according to an aspect of the invention;

FIG. 2 illustrates a catheter and introducer sheath shown in FIG. 1;

FIG. 3 is a partial cut away view of the introducer sheath of FIG. 2 carrying a guidewire assembly loaded with an occluding device;

FIG. 4 is a cross section of the guidewire assembly illustrated in FIG. 3:

FIG. 5 is a schematic view of the guidewire assembly of FIG. 4:

FIG. **6** is a second schematic view of the guidewire assembly of FIG. **4**;

FIG. 7 illustrates the occluding device and a portion of the guidewire assembly positioned outside the catheter, and how a proximal end of the occluding device begins to deploy within a vessel;

FIG. 8 illustrates a step in the method of deploying the 65 occluding device;

FIG. 9 illustrates the deployment of the occluding device according to an aspect of the present invention;

FIG. 10 is a schematic view of a guidewire assembly according to another embodiment of the present invention; and

FIG. 11 is a schematic view of the deployed occluding device after having been deployed by the guidewire assembly of FIG. 10.

DETAILED DESCRIPTION

An occluding device delivery assembly having portions with small cross section(s) and which is highly flexible is described herein. FIG. 1 illustrates an introducer sheath 10 according to an aspect of the present invention that receives, contains and delivers an occluding device 100 to a flexible micro-catheter 1 for positioning within the vasculature of an individual. The occluding device 100 can include those embodiments disclosed in copending U.S. patent application Ser. No. 11/136,395, titled "Flexible Vascular Occluding Device", filed on May 25, 2005, which is expressly hereby incorporated by reference in its entirety.

A distal end 12 of the introducer sheath 10 is sized and configured to be received within a hub 2 of the micro-catheter 1, as shown in FIGS. 1 and 2. The hub 2 can be positioned at the proximal end of the micro-catheter 1 or at another location spaced along the length of the micro-catheter 1. The microcatheter 1 can be any known micro-catheter that can be introduced and advanced through the vasculature of a patient. In an embodiment, the micro-catheter has an inner diameter of 0.047 inch or less. In another embodiment, the micro-catheter has an inner diameter of about 0.027 inch to about 0.021 inch. 30 In an alternative embodiment, the micro-catheter could have an inner diameter of about 0.025 inch. However, it is contemplated that the catheter 1 can have an inner diameter that is greater than 0.047 inch or less than 0.021 inch. After the introducer sheath 10 is positioned within the catheter hub 2, 35 the occluding device 100 can be advanced from the introducer sheath 10 into the micro-catheter 1 in preparation for deploying the occluding device 100 within the vasculature of the patient.

The micro-catheter 1 may have at least one fluid introduction port 6 located adjacent the hub 2 or at another position along its length. The port 6 is preferably in fluid communication with the distal end of the micro-catheter 1 so that a fluid, e.g., saline, may be passed through the micro-catheter 1 prior to insertion into the vasculature for flushing out air or 45 debris trapped within the micro-catheter 1 and any instruments, such as guidewires, positioned within the micro-catheter 1. The port 6 may also be used to deliver drugs or fluids within the vasculature as desired.

FIG. 3 illustrates the introducer sheath 10, an elongated 50 flexible delivery guidewire assembly 20 that is movable within the introducer sheath 10 and the occluding device 100. As shown, the guidewire assembly 20 and the occluding device 100, carried by the guidewire assembly 20, have not been introduced into the micro-catheter 1. Instead, as illustrated, they are positioned within the introducer sheath 10. The introducer sheath 10 may be made from various thermoplastics, e.g., PTFE, FEP, HDPE, PEEK, etc., which may optionally be lined on the inner surface of the sheath or an adjacent surface with a hydrophilic material such as PVP or some other plastic coating. Additionally, either surface may be coated with various combinations of different materials, depending upon the desired results.

The introducer sheath 10 may include drainage ports or purge holes (not shown) formed into the wall near the area 65 covering the occluding device 100. There may be a single hole or multiple holes, e.g., three holes, formed into introducer

4

sheath 10. These purge holes allow for fluids, e.g., saline, to readily escape from in between the introducer sheath 10 and the guidewire assembly 20 when purging the sheath prior to positioning the introducer sheath 10 in contact with the catheter hub 2, e.g., to remove trapped air or debris.

As shown in FIG. 4, the guidewire assembly 20 includes an elongated flexible guidewire 21. The flexibility of the guidewire 21 allows the guidewire assembly to bend and conform to the curvature of the vasculature as needed for positional movement of the occluding device 100 within the vasculature. The guidewire 21 may be made of a conventional guidewire material and have a solid cross section. Alternatively, the guidewire 21 can be formed from a hypotube. In either embodiment, the guidewire 21 has a diameter D₅ ranging from about 0.010 inch to about 0.020 inch. In an embodiment, the largest diameter of the guidewire is about 0.016 inch. The material used for the guidewire 21 can be any of the known guidewire materials including superelastic metals, e.g., Nitinol. Alternatively, the guidewire 21 can be formed of 20 metals such as stainless steel. Length L₄ of the guidewire can be from about 125 to about 190 cm. In an embodiment, the length L_4 is about 175 cm.

The guidewire assembly 20 can have the same degree of flexion along its entire length. In an alternative embodiment, the guidewire assembly 20 can have longitudinal sections, each with differing degrees of flexion/stiffness. The different degrees of flexions for the guidewire assembly 20 can be created using different materials and/or thicknesses within different longitudinal sections of the guidewire 21. In another embodiment, the flexion of the guidewire 21 can be controlled by spaced cuts (not shown) formed within the delivery guidewire 21. These cuts can be longitudinally and/or circumferentially spaced from each other. The cuts can be formed with precision within the delivery guidewire 21. Different sections of the delivery guidewire 21 can include cuts formed with different spacing and different depths to provide these distinct sections with different amounts of flexion and stiffness. In any of the above embodiments, the guidewire assembly 20 and the guidewire 21 are responsive to torque applied to the guidewire assembly 20 by the operator. As discussed below, the torque applied to the guidewire assembly 20 via the guidewire 21 can be used to release the occluding device 100 from the guidewire assembly 20.

The size and shape of the cuts formed within the delivery guidewire 21 may be controlled so as to provide greater or lesser amounts of flexibility. Because the cuts can be varied in width without changing the depth or overall shape of the cut, the flexibility of the delivery guidewire 21 may be selectively altered without affecting the torsional strength of the delivery guidewire 21. Thus, the flexibility and torsional strength of the delivery guidewire 21 may be selectively and independently altered.

Advantageously, longitudinally adjacent pairs of cuts may be rotated about 90 degrees around the circumference of the delivery guidewire 21 from one another to provide flexure laterally and vertically. However, the cuts may be located at predetermined locations to provide preferential flexure in one or more desired directions. Of course, the cuts could be randomly formed to allow bending (flexion) equally, non-preferentially in all directions or planes. In one embodiment, this could be achieved by circumferentially spacing the cuts.

The flexible delivery guidewire 21 can include any number of sections having the same or differing degrees of flexion. For example, the flexible delivery guidewire 21 could include two or more sections. In the embodiment illustrated in FIG. 4, the flexible delivery guidewire 21 includes three sections, each having a different diameter. Each section can have a

diameter of about 0.005 inch to about 0.025 inch. In an embodiment, the diameter of one or more sections can be about 0.010 inch to about 0.020 inch. A first section 22 includes a proximal end 23 that is located opposite the position of the occluding device 100. The first section 22 can have 5 a constant thickness along its length. Alternatively, the first section 22 can have a thickness (diameter) that tapers along its entire length or only a portion of its length. In the tapered embodiment, the thickness (diameter) of the first section 22 decreases in the direction of a second, transition section 24. For those embodiments in which the guidewire 21 has a circular cross section, the thickness is the diameter of the section.

The second, transition section 24 extends between the first section 22 and a third, distal section 26. The second section 24 tapers in thickness from the large diameter of the first section 22 to the smaller diameter of the third section 26. As with the first section 22, the second section 24 can taper along its entire length or only a portion of its length.

The third section 26 has a smaller thickness compared to 20 the other sections 22, 24 of the delivery guidewire 21. The third section 26 extends, away from the tapered second section 24 that carries the occluding device 100. The third section 26 can taper along its entire length from the second section 24 to the distal end 27 of the delivery guidewire 21. Alternatively, 25 the third section 26 can have a constant diameter or taper along only a portion of its length. In such an embodiment, the tapering portion of the third section 26 can extend from the second section 24 or a point spaced from the second section 24 to a point spaced from distal end 27 of the delivery 30 guidewire 21. Although three sections of the delivery guidewire 21 are discussed and illustrated, the delivery guidewire 21 can include more than three sections. Additionally, each of these sections can taper in their thickness (diameter) along all or only a portion of their length. In any of the 35 disclosed embodiments, the delivery guidewire 21 can be formed of a shape memory alloy such as Nitinol.

A tip 28 and flexible tip coil 29 are secured to the distal end 27 of the delivery guidewire 21 as shown in FIGS. 4 and 5. The tip 28 can include a continuous end cap or cover as shown in the figures, which securely receives a distal end of the tip coil 29. Flexion control is provided to the distal end portion of the delivery guidewire 21 by the tip coil 29. However, in an embodiment, the tip 28 can be free of the coil 29. The tip 28 has a non-percutaneous, atraumatic end face. In the illustrated embodiment, the tip 28 has a rounded face. In alternative embodiments, the tip 28 can have other non-percutaneous shapes that will not injure the vessel in which it is introduced. As illustrated in FIG. 4, the tip 28 includes a housing 45 that securely receives the distal end of the guidewire 21 within an 50 opening 46 in the interior surface of the housing 45. The guidewire 21 can be secured within the opening by any known means.

As shown in FIG. 4, the tip coil 29 surrounds a portion of the guidewire 21. The tip coil 29 is flexible so that it will 55 conform to and follow the path of a vessel within the patient as the tip 28 is advanced along the vessel and the guidewire 21 bends to follow the tortuous path of the vasculature. The tip coil 29 extends rearward from the tip 28 in the direction of the proximal end 23, as shown.

The tip **28** and coil **29** have an outer diameter D_1 of about 0.010 inch to about 0.018 inch. In an embodiment, their outer diameter D_1 is about 0.014 inch. The tip **28** and coil **29** also have a length L_1 of about 0.1 cm to about 3.0 cm. In an embodiment, they have a total length L_1 of about 1.5 cm.

A proximal end 30 of the tip coil 29 is received within a housing 32 at a distal end 24 of a protective coil 35, as shown

6

in FIGS. 1 and 4. The housing 32 and protective coil 35 have an outer diameter D2 of about 0.018 inch to about 0.038 inch. In an embodiment, their outer diameter D_2 is about 0.024 inch. The housing 32 and protective coil 35 have a length L2 of about 0.05 cm to about 0.2 cm. In an embodiment, their total length L2 is about 0.15 cm.

The housing 32 has a non-percutaneous, atraumatic shape. For example, as shown in FIG. 5, the housing 32 has a substantially blunt profile. Also, the housing 32 can be sized to open/support the vessel as it passes through it. Additionally, the housing 32 can include angled sidewalls sized to just be spaced just off the inner surface of the introducer sheath 10.

The housing 32 and protective coil 35 form a distal retaining member that maintains the position of the occluding device 100 on the flexible guidewire assembly 20 and helps to hold the occluding device 100 in a compressed state prior to its delivery and deployment within a vessel of the vasculature. The protective coil 35 extends from the housing 32 in the direction of the proximal end 23 of the delivery guidewire 21, as shown in FIG. 4. The protective coil 35 is secured to the housing 32 in any known manner. In a first embodiment, the protective coil 35 can be secured to the outer surface of the housing 32. In an alternative embodiment, the protective coil 35 can be secured within an opening of the housing 32 so that the housing 32 surrounds and internally receives the distal end 51 of the protective coil 35 (FIG. 4). As shown in FIGS. 3 and 4, the distal end 102 of the occluding device 100 is retained within the proximal end 52 so that the occluding device 100 cannot deploy while positioned in the sheath 10 or the micro-catheter 1.

At the proximal end of the occluding device 100, a bumper coil 60 and cap 62 prevent lateral movement of the occluding device 100 along the length of the guidewire 21 in the direction of the proximal end 23, see FIG. 3. The bumper coil 60 and cap 62 have an outer diameter D₄ of about 0.018 inch to about 0.038 inch. In an embodiment, their outer diameter D₄ is about 0.024 inch. The cap 62 contacts the proximal end 107 of the occluding device 100 and prevents it from moving along the length of the guidewire 21 away from the protective coil 35. The bumper coil 60 can be in the form of a spring that contacts and pressures the cap 62 in the direction of the protective coil 35, thereby creating a biasing force against the occluding device 100. This biasing force (pressure) aids in maintaining the secured, covered relationship between the distal end 102 of the occluding device 100 and the protective coil 35. As with any of the coils positioned along the delivery guidewire 21, the bumper coil 60 can be secured, to the delivery guidewire 21 by soldering, welding, RF welding, glue, and/or other known adhesives.

In an alternative embodiment illustrated in FIG. 10, the bumper coil 60 is not utilized. Instead, a proximal end 107 of the occluding device 100 is held in position by a set of spring loaded arms (jaws) 104 while positioned within the introducer sheath 10 or the micro-catheter 1. The inner surfaces of the micro-catheter 1 and the introducer sheath 10 limit the radial expansion of the arms 104. When the proximal end of the occluding device passes out of the micro-catheter 1, the arms 104 would spring open and release the occluding device as shown in FIG. 11.

In an alternative embodiment, the bumper coil 60 and cap 62 can be eliminated and the proximal end of the occluding device 100 can be held in position relative to the protective coil 35 by a tapered section of the guidewire 21. In such an embodiment, the enlarged cross section of this tapered section can be used to retain the occluding device 100 in position

along the length of the delivery guidewire 21 and prevent movement of the occluding device 100 in the direction of the proximal end 23.

As shown in FIG. 4, the guidewire assembly 20 includes a support 70 for the occluding device 100. In a first embodiment, the support 70 can include an outer surface of the delivery guidewire 21 that is sized to contact the inner surface of the occluding device 100 when the occluding device 100 is loaded on the guidewire assembly 20. In this embodiment, the outer surface of the delivery guidewire 21 supports the occluding device 100 and maintains it in a ready to deploy state. In another embodiment, illustrated in the Figures, the support 70 comprises a mid-coil 70 that extends from a location proximate the protective coil 35 rearward toward the bumper coil 60. The mid-coil 70 extends under the occluding device 100 and over the delivery guidewire 21, as shown in FIG. 1. The mid-coil 70 can be coextensive with one or more sections of the delivery guidewire 21. For example, the midcoil 70 could be coextensive with only the second section 24 20 of the delivery guidewire 21 or it could extend along portions of both the third section 26 and the second section 24 of the delivery guidewire 21.

The mid-coil 70 provides the guidewire assembly 20 with an outwardly extending surface that is sized to contact the 25 inner surface of the occluding device 100 in order to assist in supporting the occluding device and maintaining the occluding device 100 in a ready to deploy state. Like the other coils discussed herein and illustrated in the figures, the coiled form of the mid-coil 70 permits the mid-coil 70 to flex with the delivery guidewire 21 as the delivery guidewire 21 is advanced through the vasculature of the patient. The mid-coil 70 provides a constant diameter along a length of the delivery guidewire 21 that is covered by the occluding device 100 regardless of the taper of the delivery guidewire 21 beneath 35 the occluding device 100. The mid-coil 70 permits the delivery guidewire 21 to be tapered so it can achieve the needed flexibility to follow the path of the vasculature without compromising the support provided to the occluding device 100. The mid-coil **70** provides the occluding device **100** with con-40 stant support regardless of the taper of the delivery guidewire 21 prior to the occluding device 100 being deployed. The smallest diameter of the occluding device 100 when in its compressed state is also controlled by the size of the mid-coil 70. Additionally, the diameter of the mid-coil 70 can be cho-45 sen so that the proper spacing, including no spacing, is established between the occluding device 100 and the inner wall of the micro-catheter 1 prior to deployment of the occluding device 100. The mid-coil 70 can also be used to bias the occluding device 100 away from the delivery guidewire 21 50 during its deployment.

In either embodiment, the support 70 can have an outer diameter D_3 of about 0.010 inch to about 0.018 inch. In an embodiment, the outer diameter D_3 is about 0.014 inch. The support 70 can also have a length L_3 of about 2.0 cm to about 55 30 cm. In an embodiment, the length L_3 of the support 70 is about 7 cm.

The occluding device 100 may also be placed on the midcoil 70 between an optional pair of radio-opaque marker bands located along the length of the guidewire assembly 20. 60 Alternatively, the protective coil 35, bumper coil 60 and or mid-coil 70 can include radio-opaque markers. In an alternative embodiment, the guidewire assembly 20 may include only a single radio-opaque marker. The use of radio-opaque markers allows for the visualization of the guidewire assembly 20 and the occluding device 100 during placement within the vasculature. Such visualization techniques may include

8

conventional methods such as fluoroscopy, radiography, ultra-sonography, magnetic resonance imaging, etc.

The occluding device 100 can be delivered and deployed at the site of an aneurysm A according to the following method and variations thereof. The delivery of the occluding device 100 includes introducing the micro-catheter 1 into the vasculature until it reaches a site that requires treatment. The micro-catheter 1 is introduced into the vasculature using a conventional technique such as being advanced over or simultaneously with a conventional vascular guidewire (not shown). The positioning of the micro-catheter 1 can occur before it receives the guidewire assembly 20 or while it contains the guidewire assembly 20. The position of the micro-catheter 1 within the vasculature can be determined by identifying radio-opaque markers positioned on or in the micro-catheter 1.

After the micro-catheter 1 is positioned at the desired location, the guidewire is removed and the distal end of the introducer sheath 10 is inserted into the proximal end of the microcatheter 1, as shown in FIG. 1. In an embodiment, the distal end of the introducer sheath 10 is introduced through the hub 2 at the proximal end of the micro-catheter 1. The introducer sheath 10 is advanced within the micro-catheter 1 until a distal tip of the introducer sheath 10 is wedged within the micro-catheter 1. At this position, the introducer sheath 10 cannot be advanced further within the micro-catheter 1. The introducer sheath 10 is then securely held while the delivery guidewire assembly 20 carrying the occluding device 100 is advanced through the introducer sheath 10 until the occluding device 100 is advanced out of the introducer sheath 10 and into the micro-catheter 1.

The guidewire assembly 20 and the occluding device 100 are advanced through the micro-catheter 1 until the tip coil 29 is proximate the distal end of the micro-catheter 1. At this point, the position of the micro-catheter 1 and guidewire assembly 20 can be confirmed. The guidewire assembly 20 is then advanced out of the micro-catheter 1 and into the vasculature of the patient so that the proximal end 107 of the occluding device 100 is positioned outside the distal end of the micro-catheter 1 and adjacent the area to be treated. At any point during these steps, the position of the occluding device 100 can be checked to determine that it will be deployed correctly and at the desired location. This can be accomplished by using the radio-opaque markers discussed above.

When the distal end 102 of the occluding device 100 is positioned outside the micro-catheter 1, the proximal end 107 will begin to expand, in the direction of the arrows shown in FIG. 7, within the vasculature while the distal end 102 remains covered by the protective coil 35. When the occluding device 100 is in the proper position, the delivery guidewire 21 is rotated (See FIG. 8) until the distal end 102 of the occluding device 100 moves away from the protective coil 35 and expands within the vasculature at the desired location. The delivery guidewire 21 can be rotated either clockwise or counter clockwise as needed to deploy the occluding device 100. In an embodiment, the delivery guidewire 21 may be rotated, for example, between two and ten turns in either or both directions. In another example, the occluding device may be deployed by rotating the delivery guidewire 21 clockwise for less than five turns, for example, three to five turns. After the occluding device 100 has been deployed, the delivery guidewire 21 can be retracted into the micro-catheter 100 and removed form the body.

In an alternative or additional deployment step shown in FIG. 9, friction between the occluding device 100 and inner surface of the micro-catheter 1 cause the distal end of the occluding device 100 to separate from the protective coil 35.

The friction can be created by the opening of the occluding device 100 and/or the mid-coil 70 biasing the occluding device 100 toward the inner surface of the micro-catheter 1. The friction between the micro-catheter 1 and the occluding device 100 will assist in the deployment of the occluding device 100. In those instances when the occluding device 100 does not open and separate from the protective coil 35 during deployment, the friction between occluding device 100 and the inner surface of the micro-catheter 1 will cause the occluding device 100 to move away from the protective coil 10 35 as the delivery guidewire 21 and the micro-catheter 1 move relative to each other. The delivery guidewire 21 can then be rotated and the occluding device 100 deployed within the vessel.

After the occluding device 100 radially self-expands into 15 gentle, but secure, contact with the walls of the vessel so as to occlude the neck of the aneurysm A, the micro-catheter 1 may be removed entirely from the body of the patient. Alternatively, the micro-catheter 1 may be left in position within vasculature to allow for the insertion of additional tools or the 20 application of drugs near the treatment site.

Known materials can be used in the present invention. One common material that can be used with the occluding device 100 and the guidewire 21 is Nitinol, a nickel-titanium shape memory alloy, which can be formed and annealed, deformed 25 at a low temperature, and recalled to its original shape with heating, such as when deployed at body temperature in the body. The radio-opaque markers can be formed of radio-opaque materials including metals, such as platinum, or doped plastics including bismuth or tungsten to aid in visualization.

The apparatus and methods discussed herein are not limited to the deployment and use within the vascular system but may include any number of further treatment applications. Other treatment sites may include areas or regions of the body such as organ bodies. Modification of each of the above-described apparatus and methods for carrying out the invention, and variations of aspects of the invention that are obvious to those of skill in the art are intended to be within the scope of the claims. Furthermore, no element, component or method step is intended to be dedicated to the public regardless of whether the element, component or method step is explicitly recited in the claims.

What is claimed:

- 1. A method for delivering a stent to a location within a vessel, said method comprising:
 - introducing a delivery assembly into a catheter, the delivery assembly comprising (i) an elongate flexible member; and (ii) a retaining member, at a distal portion of the 50 elongate member, having an inner lumen that extends around a circumference of the elongate member, the lumen receiving a first end of the stent to secure a portion of the stent in the retaining member;
 - positioning the stent and a distal end of the catheter proximate an aneurysm within the vessel such that at least a portion of the stent is outside of the distal end of the catheter;
 - rotating said retaining member relative to the stent, whereby the first end moves proximally relative to the 60 retaining member and is disengaged from within the lumen while deploying said stent at the aneurysm.
- 2. The method according to claim 1, further comprising the step of removing the delivery assembly from within the catheter
- 3. The method according to claim 1, further comprising the step of removing the catheter from within the vessel.

10

- **4**. The method according to claim **1**, further comprising the step of confirming the position of said stent prior to deploying said stent.
- 5. The method according to claim 1, wherein the stent is self-expanding.
- **6**. The method according to claim **1**, wherein the retaining member comprises a protective coil.
- 7. The method according to claim 1, further comprising limiting proximal movement of a second end of the stent along a length of the elongate member.
- 8. The method according to claim 1, wherein the first end of the stent is biased radially outwardly against the retaining member.
- 9. The method according to claim 1, wherein the delivery assembly further comprises a proximal member configured to limit proximal movement of a second end of the stent along a length of the flexible member, the method further comprising maintaining the retaining member and the proximal member substantially fixed axially with respect to each other while the stent is released from the lumen.
- 10. A method for positioning a self-expanding device at a treatment site in a vessel, the method comprising:
 - introducing a catheter and a delivery assembly into the vessel, the delivery assembly comprising an elongate flexible member including a retaining member receiving a first end of the self-expanding device, the self-expanding device being concentrically within the retaining member and biased against a surface positioned about a lumen of the retaining member; and
 - positioning the catheter and the delivery assembly such that the retaining member and at least a portion of the self-expanding device are outside a distal end of the catheter and such that a second end of the self-expanding device is expanded toward a wall of the vessel;
 - rotating the retaining member so as to release the first end of the self-expanding device from the retaining member by moving the first end proximally relative to the retaining member.
- 11. The method according to claim 10, wherein the treatment site comprises an aneurysm.
- 12. The method according to claim 10, wherein the retaining member comprises a protective coil, and the self-expanding device is received within an interior of the protective coil.
- 13. The method according to claim 10, further comprising removing the delivery assembly proximally through the catheter and leaving the self-expanding device in the vessel.
- **14**. A method for delivering a self-expanding device in a body lumen, the method comprising:
 - providing a delivery assembly positioned at least partially within an introducer sheath, the delivery assembly comprising an elongate flexible member and a retaining member at a distal portion of the delivery assembly, the elongate flexible member extending through the retaining member, the retaining member having a lumen therein extending around the elongate flexible member, the retaining member receiving a first end of the self-expanding device within the lumen, the self-expanding device being biased radially outward against the retaining member;
 - advancing at least a portion of the delivery assembly through the introducer sheath and into a catheter;
 - positioning the delivery assembly and the catheter at least partially within the body lumen such that the retaining member is outside a distal end of the catheter and at least a portion of the self-expanding device extends distal of

the distal end of the catheter and such that a second end of the self-expanding device is expanded toward a wall of the body lumen;

rotating the retaining member, whereby the first end moves proximally relative to the retaining member so as to 5 release the first end from within the retaining member.

- **15**. The method according to claim **14**, wherein the assembly further comprises a second retaining member receiving a second end of the self-expanding device, the method further comprising releasing the second end of the self-expanding 10 device from the second retaining member.
- 16. The method according to claim 14, wherein the retaining member comprises a protective coil, the self-expanding device received within an interior of the protective coil.
- 17. The method according to claim 14, further comprising 15 inserting a distal end of the introducer sheath into a proximal end of the catheter, and removing the introducer sheath from the catheter after advancing the delivery assembly through the introducer sheath into the catheter.
- **18**. The method according to claim **14**, further comprising 20 removing the delivery assembly proximally through the catheter and leaving the self-expanding device in the body lumen.

* * * * *